

The multi-tier structure of patterning networks increases access to positional information

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In pattern-forming developmental systems, cells commonly interpret graded input signals, known as morphogens. Morphogens often pattern tissues through cascades of sequential gene expression steps. Such a multi-tiered structure appears to constitute suboptimal use of the positional information provided by the input morphogen because noise is added at each tier. However, the conventional theory neglects the role of the format in which information is encoded. We argue that the relevant performance measure is not solely the amount of information carried by the morphogen, but the amount of information that can be *accessed* by the downstream network. We demonstrate that quantifying the information that is accessible to the system naturally explains the prevalence of multi-tiered network architectures as a consequence of the noise inherent to the control of gene expression. We support our argument with empirical observations from patterning along the major body axis of the fruit fly embryo.

Keywords: noise / genetic regulation / developmental biology / *Drosophila*

Survival of living systems requires reliable function in the presence of environmental fluctuations and molecular stochasticity, often termed noise. Much theoretical work has been devoted to discovering features of biological networks that permit living systems to function correctly under noisy conditions. Examples of such features include kinetic proof-reading [1, 2], network motifs that confer robustness [3, 4], and feedback [5]. The context of embryonic development offers an especially promising setting for investigating principles of network design because for a complex multicellular organism, the reliability of its developmental program directly determines the probability of reaching reproductive age. Therefore, low error rate and/or high error tolerance are likely to be key determinants of the structures of developmental circuits [6, 7].

In many developing embryonic systems, cellular identities are conferred by graded input signals that induce dose-dependent gene expression programs as outputs [8, 9]. Such graded inputs, termed morphogens, often function as diffusible molecules produced by a localized expression source [10, 11]. Localized expression generates concentration gradients in a field of otherwise naive and identical cells (presented in simplified form as a one-dimensional array in Fig. 1). Cells activate specific expression programs in response to the local morphogen concentration $c(x)$. When c correlates closely with distance x from the source, such gradients carry a large amount of “positional information” [12] quantified via the mutual information $I[c(x), x]$ [13, 14]. In principle, a morphogen gradient carrying sufficient information could induce in each cell the gene expression program appropriate for its position, thus generating the required spa-

tial arrangement of cell fates [15] (Fig. 1A). In the most straightforward model, assuming the input morphogen is sufficiently reproducible [16], local morphogen concentration is directly interpreted by each cell, i.e., the local input activates all genes required at a given position, with no additional cycles of gene expression modulation. A central tenet of information theory, the information processing inequality, states that each transmission or processing step can only reduce the total information contained in a signal. Direct decoding might

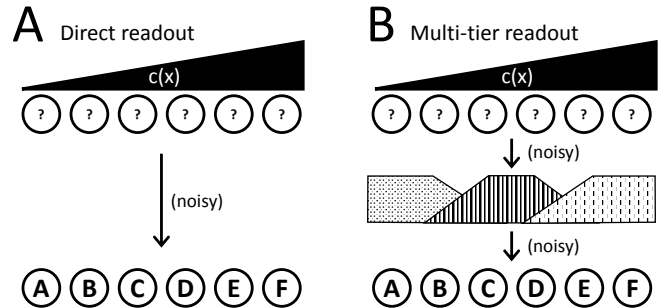


FIG. 1. Direct versus multi-tiered decoding strategies for gradient-mediated patterning. (A) Direct decoding: to reduce noise introduced by intrinsically variable gene expression, patterning proceeds through a single cycle of transcription and translation. Differences in morphogen input $c(x)$ directly specify gene expression programs A-F along axis x . (B) Multi-tiered decoding: morphogen first elicits expression of short range diffusible factors in domains spanning several cells. These gene products then induce programs A-F through a second cycle of transcription/translation. The added step introduces additional gene expression noise, reducing patterning information compared to direct decoding (A).

therefore be expected to dominate in early development as the optimal strategy for transmitting positional information. This expectation seems all the more valid given the widespread observation that the processes of transcription and translation exhibit considerable intrinsic variability, or noise [17, 18]. Thus information loss in gene regulatory processes should be particularly notable.

Therefore, from the perspective of information theory, it is surprising that many gradient-based systems exhibit a multi-tiered architecture in which reiterated cycles of transcription and translation are required to attain patterning goals (illustrated in Fig. 1B). For example, in the vertebrate central nervous system, the unpatterned neuroectoderm exhibits a graded distribution of multiple diffusible signaling molecules. These signals subdivide the prospective brain into relatively large fore-, mid-, and hindbrain territories, which are then segmented into smaller subunits by additional signaling activity [19–21]. Similar patterns of broad subdivision followed by short-range refinement are found during the specification of the vertebrate neural crest by reiterated rounds of extracellular signaling [22]; in the formation of segmented muscle precursors (somites) by FGF and Notch followed by short range Ephrin activity [23, 24]; the dorsal-ventral patterning of the *Drosophila* body axis, first by a gradient of NF- κ B activity (also called Dorsal) and then by members of the BMP family of secreted signaling molecules [25, 26]; and also in the fruit fly, the patterning of the anterior-posterior (AP) axis by gradients of diffusible transcription factors within the shared cytoplasm of the nuclear syncytium [15, 27, 28].

These examples and others illustrate a common theme where long range signaling gradients subdivide a large field into smaller domains, within which the patterned expression of secondary factors establishes elaborated patterns (Fig. 1B). Since each cycle of transcription and translation introduces more noise, the widespread use of the multi-tiered architecture appears to conflict with the expectation that development should favor circuits exhibiting efficient information utilization.

This apparent conflict arises because Shannon’s information content of a signal [13] has two important limitations that are commonly underappreciated in biological applications of information theory. First, the information content of a patterning cue or other biological signal is defined locally in space and time, whereas its interpretation is non-local, and instead occurs over time and frequently involves diffusive signals. For this reason, the naive application of information processing inequality in these systems is incorrect, and the local, instantaneous information content in a signal does not in fact provide an upper bound for the performance of downstream processes interpreting this signal [29]. Second, the same amount of information can be encoded in formats that are more or less easy for the system to access, since the interpreting circuit is itself subject to noise. Thus, the

local information content of a signal is neither an upper bound nor a fair estimate of the amount of information this signal can “transmit” to the downstream circuit.

Here we use a simplified model to illustrate these limitations of what we call “raw” information content, contrasting it with “accessible information” that we introduce. We show how the advantages of a multi-tiered architecture can be understood from first principles, as a tradeoff between information content and accessibility, and support our reasoning with experiments on the well-studied segmentation gene network responsible for anterior-posterior patterning in the *Drosophila* embryo.

Results

An abstract gradient response problem. A one-dimensional array of cells i located at positions ($0 < x_i < L$) is exposed to a noisy linear gradient of an input morphogen $c(x)$ spanning the range $[0, c_{\max}]$. To build intuition, we will assume the noise of input $c(x)$ to be Gaussian, of constant magnitude σ_0 , and uncorrelated between cells: $c(x_i) \equiv c_i = (x_i/L) c_{\max} + \sigma_i$, where σ_i are i.i.d., drawn from a Gaussian of width σ_0 (Fig. 2A). Cells respond to morphogen $c(x)$ by modulating gene expression through intrinsically noise-prone signal transduction and transcription/translation processes. We will model this response as a composition of three steps, three elementary operations that constitute the “toolkit” with which cells can access and process information contained in patterning cues: *access*, *amplify*, and *average*.

Let g^{out} be a gene product whose expression is controlled by $c(x)$. The simplest readout is achieved by placing gene g^{out} under the control of a promoter that is responsive to c and by accumulating the output protein for some time τ . In our model, we express the amount of g^{out} produced during this time by a cell i as $g_i^{\text{out}} = F(c_i^{\text{est}})$, where c_i^{est} is a noisy estimate of the true concentration c_i that the system could obtain in time τ (“access”), and F is some deterministic input-output function (“amplify”); for simplicity, we first consider F to be pure linear amplification with coefficient λ , denoted F_λ . The “access” operation is the key element of our framework. Specifically, we write

$$c_i^{\text{est}} = c_i + \eta_i,$$

where η_i reflects the intrinsic stochasticity of transcription and, in principle, many other noise sources. Here we will model η_i simply as being drawn from a Gaussian distribution of width η_0 . In other words, we postulate that each “access” operation takes time τ and comes at the price of corrupting the signal with extra noise of magnitude η_0 .

The final toolkit operation is averaging. Because pat-

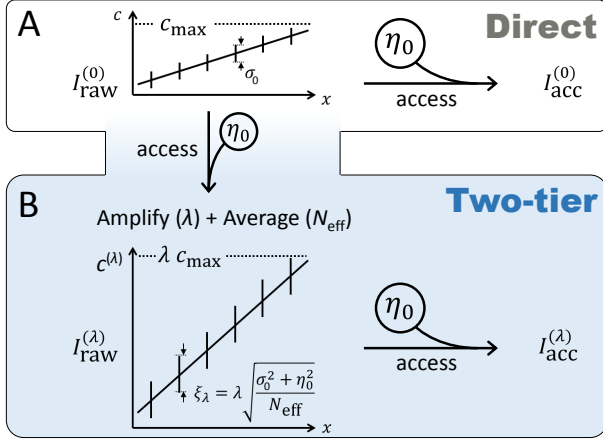


FIG. 2. **The two patterning strategies.** **A:** In the direct strategy, target genes are controlled directly by c . **B:** The two-tier strategy involves a second patterning factor $c^{(\lambda)}$; target genes are separated from the input by two tiers of “access” operations. Left, raw information content. Right, accessible information content.

ternary systems typically act over durations that are long (hours) compared to the time required to synthesize mRNA and protein (minutes), cells can perform temporal averaging by allowing stable gene products to accumulate [31]: if T is the time available for patterning, the system can effectively perform T/τ access operations. In addition, the production of soluble factors that can be shared between cells gives rise to spatial averaging [30, 31]. Both types of averaging offer the system some capacity to perform multiple measurements of the input, which we capture formally by an averaging operator $G_{N_{\text{eff}}}$. Here N_{eff} indicates the effective number of independent measurements, so that application of $G_{N_{\text{eff}}}$ to a morphogen, by definition, reduces expression fluctuations by a factor $1/N_{\text{eff}}$.

We distinguish between two patterning strategies. In the first (“direct strategy”; Fig. 2A), cell-fate-specific target genes are controlled directly by c and no other patterning factors are involved. Any available averaging mechanisms are applied to c itself. In the second (“two-tier”) strategy, cells perform an amplifying readout of c with input-output function F_λ to establish a spatial profile of a second factor $c^{(\lambda)}$ (Fig. 2B). The patterning time T is spent on accumulating and averaging $c^{(\lambda)}$. Mathematically, in the two scenarios, the cell-fate-specific target genes are controlled by:

$$c^{(0)} = G_{N_{\text{eff}}}[c] \quad (\text{direct strategy}) \quad (1)$$

$$c^{(\lambda)} = G_{N_{\text{eff}}}[F_\lambda(c + \eta)] \quad (\text{two-tier strategy}) \quad (2)$$

We now ask: when, if ever, does the noisy amplification step of the two-tier strategy provide a benefit to the system?

Standard information-theoretic considerations do not explain the benefits of amplification. The positional information carried by a linear morphogen $c(x)$ with dynamic range $c_{\max}$ and noise σ_0 , which we call the “raw information content” of a gene expression profile, is given by

$$I_{\text{raw}}[c(x), x] = \ln \left(\frac{c_{\max}}{\sigma_0 \sqrt{2\pi e}} \right)$$

(see Supplementary Information). It depends only on the ratio $\phi = c_{\max}/\sigma_0$; for convenience, we define $\mathcal{I}(\phi) \equiv \ln \left(\frac{\phi}{\sqrt{2\pi e}} \right)$, which is an increasing function of ϕ .

Let us compare the two patterning strategies from the point of view of the raw information content carried by the controlling signal. In the direct strategy (1), the application of $G_{N_{\text{eff}}}$ reduces the input noise to $\sigma_0/\sqrt{N_{\text{eff}}}$ and so the controlling signal $c^{(0)}$ carries $I_{\text{raw}}^{(0)} = \mathcal{I} \left(\frac{c_{\max}}{\sigma_0/\sqrt{N_{\text{eff}}}} \right)$ bits of raw information. In the two-tier strategy (2), the amplified profile $c^{(\lambda)}$ is characterized by noise $\xi_\lambda = \lambda \sqrt{\frac{\sigma_0^2 + \eta_0^2}{N_{\text{eff}}}}$, and its raw information content is therefore

$$I_{\text{raw}}^{(\lambda)} = \mathcal{I} \left(\frac{\lambda c_{\max}}{\xi_\lambda} \right) = \mathcal{I} \left(c_{\max} \sqrt{\frac{N_{\text{eff}}}{\sigma_0^2 + \eta_0^2}} \right) < I_{\text{raw}}^{(0)}. \quad (3)$$

Averaging mitigates the loss of positional information when using a noisy readout [30]. If N_{eff} is sufficiently large, the amplified and averaged profile carries even more information than the original input. (Note that the information processing inequality is not violated, as it states only that the output cannot carry more information than N_{eff} independent copies of the input.) Nevertheless, applying averaging directly to the input (the direct strategy) always yields more raw information; thus, the multi-step scenario appears inferior to a direct readout.

In real systems, the three operations we treat as independent may be mechanistically linked. For example, if $c(x)$ is an intracellular factor while spatial averaging requires a small diffusible molecule, then performing an extra readout can provide access to an otherwise unavailable averaging mechanism. By assuming that the two strategies (1) and (2) can benefit from equal amounts of averaging, which in our model simply reduces expression noise and is obviously beneficial, we can focus specifically on the effect of signal amplification. Multi-tier patterning proceeds through rounds of amplification: small differences in input result in large differences in gene expression so as to establish increasingly sharp boundaries delimiting expression domains [32], yet in our expression (3) for the information content of the amplified profile $c^{(\lambda)}$, the amplification factor λ cancels out. Thus, considerations based on raw information content fail to explain the prevalence of signal amplification.

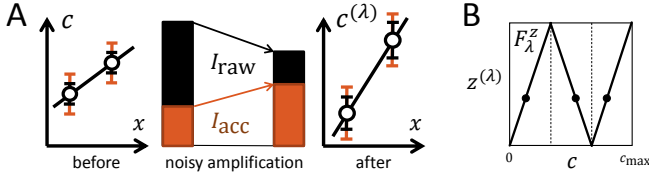


FIG. 3. **A:** Noisy amplification can increase accessible information even if raw information is reduced. Inner error bars are the signal variability and increase when amplification adds new noise, reducing I_{raw} . Outer error bars represent the signal observed by the noisy cell machinery (corrupted by noise η_0). After amplification, the relative importance of η_0 is reduced, increasing I_{acc} . **B:** The “segmentation” input-output function F_{λ}^z for integer λ (here $\lambda = 3$) preserves the dynamic range of morphogen concentration. Locations such as those indicated by dots now have identical expression levels of $z^{(\lambda)}$ (the y axis), but can be distinguished using the input morphogen c (the x axis on this plot).

The benefits of the multi-tiered strategy lie in making the “raw” information more accessible. The benefits of amplification and the advantages of the multi-tier strategy become clear when we observe that, due to the intrinsic noise in the regulatory readout, the raw information content is an inadequate measure of a morphogen’s usefulness to the system. The purpose of a morphogen is to activate downstream processes; the relevant quantity is therefore not the amount of information a morphogen carries, but the amount of information it can transmit to its downstream targets. Since biological control is intrinsically noisy, the two quantities are distinct.

Our model was designed to make this particularly clear: since the system can never access the true concentration c , but only a noisy estimate c^{est} , $I_{\text{raw}}[c]$ is beyond the system’s reach. We define *accessible* information in a morphogen I_{acc} as the amount of information the system can access in time τ :

$$I_{\text{acc}}[c] \equiv I_{\text{raw}}[c^{\text{est}}] = I_{\text{raw}}[c + \eta], \quad (4)$$

where η , again, is a Gaussian noise of magnitude η_0 within our model.

The amount of accessible information provided by the direct strategy (Fig. 2B) is given by

$$I_{\text{acc}}^{(0)} = \mathcal{I} \left(\frac{c_{\text{max}}}{\sqrt{\frac{\sigma_0^2}{N_{\text{eff}}} + \eta_0^2}} \right) \quad (5)$$

whereas for the amplified profile $c^{(\lambda)}$ it is

$$I_{\text{acc}}^{(\lambda)} = \mathcal{I} \left(\frac{\lambda c_{\text{max}}}{\sqrt{\lambda^2 \frac{\sigma_0^2}{N_{\text{eff}}} + \eta_0^2}} \right) = \mathcal{I} \left(\frac{c_{\text{max}}}{\sqrt{\frac{\sigma_0^2}{N_{\text{eff}}} + \frac{\eta_0^2}{\lambda^2}}} \right). \quad (6)$$

The amplification factor λ no longer cancels out in (6); amplifying dynamic range is beneficial, since it reduces

the relative importance of the intrinsic readout noise (Fig. 3A). Comparing (5) and (6), we find that the extra tier of noisy amplification is beneficial if and only if

$$\eta_0^2 \left(1 - \frac{1}{N_{\text{eff}}} - \frac{1}{\lambda^2} \right) > 0 \quad (7)$$

Note that the condition (7) is never satisfied if $N_{\text{eff}} = 1$ (no averaging) or $\lambda = 1$ (no amplification). Intuitively, our argument demonstrates that the patterning system is a mechanism that invests some effort into making a careful measurement ($N_{\text{eff}} > 1$) and encodes this information in a more accessible format where steeper concentration changes ($\lambda > 1$) can be interpreted with a faster, and therefore noisier readout. This mechanism is useful precisely because regulatory readout is intrinsically noisy, otherwise direct readout would have been the better strategy.

Multiple tiers improve gradient interpretation even when raw information decreases. So far we considered the information content (raw or accessible) in each tier separately. However, in principle, downstream processes could access all patterning cues and not simply the final tier. As a result, extra readout tiers can be beneficial even when they carry very little information on their own.

To see this, consider the input-output function F_{λ}^z depicted in Fig. 3B. In some respects, it is more realistic than the purely amplifying linear readout F_{λ} considered above, since real patterning systems must operate within a limited global dynamic range of morphogen concentrations. Let $z^{(\lambda)}$ be the morphogen profile established by the new F_{λ}^z -shaped readout of c ; it has noise magnitude ξ_{λ} (same as the noise in $c^{(\lambda)}$), but is folded onto itself λ times, reminiscent of the spatially reiterated expression of genes involved in *Drosophila* axis segmentation. Repeatedly using the same output values at multiple positions naturally reduces mutual information between the output concentration and position:

$$I_{\text{raw}}[z^{(\lambda)}] = I_{\text{raw}}[c^{(\lambda)}] - \ln \lambda; \quad I_{\text{acc}}[z^{(\lambda)}] = I_{\text{acc}}[c^{(\lambda)}] - \ln \lambda.$$

However, the λ locations with identical concentrations of $z^{(\lambda)}$ are made distinguishable by the original morphogen c (Fig. 3B). Therefore, the *joint* information that the original and the amplified profiles together provide about a cell’s location is the same for F_{λ}^z as it was for F_{λ} :

$$I[\{c, z^{(\lambda)}\}, x] = I[\{c, c^{(\lambda)}\}, x]$$

Replacing information content of a single profile by this joint information, our argument demonstrating that amplification increases accessible information can now be repeated verbatim [33], and we again find that the extra readout is beneficial as long as (7) is satisfied. Note,

however, that on its own, $z^{(\lambda)}$ may carry *less* information than the original morphogen c . The easiest way to see this is to compare their noise levels:

$$\left(\frac{\xi_\lambda}{\sigma_0}\right)^2 = \frac{\lambda^2}{N_{\text{eff}}} \left(1 + \frac{\eta_0^2}{\sigma_0^2}\right)$$

If the effect of amplification is stronger than that of averaging, we find $\xi_\lambda/\sigma_0 > 1$. In this scenario, the amplified profile $z^{(\lambda)}$ has the same dynamic range but lower precision than the original morphogen c , and therefore, on its own, carries less information (whether raw or accessible). This shows how a decrease in noise from input to output is unnecessary to explain how systems can benefit from multi-tiered interpretation. Importantly, patterning is enhanced even in cases where intermediate steps increase noise.

Multiple tiers enhance early segment patterning in *Drosophila*. In this system, segmentation of the AP axis proceeds through four tiers of gene activity, termed maternal gradients, gap genes, pair-rule genes, and segment polarity genes [28]. The sequential activity of each tier subdivides the naive blastoderm into smaller domains of gene expression with increasingly sharp boundaries, culminating in the designation of each row of cells with its own unique set of expressed genes (Fig. 4A). This process is subject to transcriptional noise with a large intrinsic component [31], as well as several other noise sources with different signatures [34–37]. No single value of η_0 adequately characterizes such readout noise. Nevertheless, we can gain important insight by computing $I_{\text{acc}}^{\eta_0}[c]$ as a function of η_0 , treating it as a variable parameter: the decay of $I_{\text{acc}}^{\eta_0}[c]$ with η_0 characterizes the tolerance to added noise of the information encoded in the morphogen (or set of morphogens) c . Applied to gene expression data from the early *Drosophila* segmentation gene network, this analysis will show how our simple model explains the use of multi-tier gradient interpretation in a real system (Fig. 4).

We focus on a particular node in this network whereby, in early embryos, two gap genes, *hb* and *Kr*, regulate a pair-rule gene *eve*. For $0.37 < x_{\text{AP}} < 0.47$, where *Kr* and *hb* expression form opposing boundaries, they are jointly responsible for creating the trough between *eve* stripes 2 and 3; other inputs to *eve* are negligible in this region at this time [38, 39]. Protein levels are measured simultaneously in each nucleus by a triple immunostaining experiment (Fig. 4A) in $N = 8$ single embryos. We determine the expression noise of each gene by comparing levels in a given nucleus with those of its immediate dorsal and ventral neighbors (see Methods).

In the defined region of interest, *eve* expression noise is higher than the respective noise in *hb* or *Kr* expression (Fig. 4B). The information content of *eve* must therefore be lower than that carried by either of its two inputs. Due

to the curvature of the embryo (Fig. 4A), the positional information of a real morphogen is only approximately related to that derived from projection onto the imaginary AP axis. Therefore, to estimate the information content for each of the three genes, we consider “idealized” Gaussian-noise profiles (panel C) with mean and noise obtained by smoothing the measured values in real embryos. The idealized profiles are normalized to the same maximum and are, by construction, functions of x_{AP} carrying positional information $I(c(x_{\text{AP}}), x_{\text{AP}})$. Restricted to the region of interest, the information content of *Hb* and *Kr* is respectively 2.6 and 2.7 bits, whereas the larger noise of *Eve* reduces its information content to only 2.0 bits. Why, then, does the system use *Eve* to regulate downstream processes, rather than utilizing *Kr* and *Hb* directly?

The answer becomes clear when we consider the accessibility of information encoded in these morphogens, namely $I_{\text{acc}}^{\eta_0}$ as a function of η_0 (panel D). A patterning strategy lacking *Eve* can access only *Hb* and *Kr*. Even if some hypothetical filtering mechanism could reduce their expression noise to arbitrarily low level, the readout noise magnitude $\eta_0 > 0$ imposes an upper bound that $I_{\text{acc}}^{\eta_0}[c_{\text{Hb}}, c_{\text{Kr}}]$ must satisfy. This corresponds to the information in a hypothetical pair of noiseless *Hb* and *Kr* and cannot be achieved in practice; it is a theoretical best-case scenario for any strategy lacking *Eve*.

When the readout noise η_0 is zero, $I_{\text{acc}}^{\eta_0}$ coincides with the raw information content, which for perfectly noiseless *Hb* and *Kr* would be infinite. However, as readout noise increases, the performance bound becomes finite and drops quickly (black curve). This behavior contrasts with the joint accessible information of the triplet (*Hb*, *Kr*, *Eve*) (magenta) as calculated using the actual measured noise of each of the three profiles. The accessible information content in the triplet is, of course, always finite, but it is also more tolerant to readout noise: due to the steeper slopes of the *Eve* profile, as η_0 increases, the accessible information content of the triplet (*Hb*, *Kr*, *Eve*) decreases slowly; importantly, more slowly than the black curve. Therefore, a crossing point is observed, whose presence does not qualitatively depend on the specifics of the readout noise model (e.g. absolute noise magnitude can be replaced by fractional). Remarkably, although *Eve* is measurably noisier than either of its inputs, its presence enables the system to access more information than could have been extracted from *Hb* and *Kr* alone, even if these inputs could be rendered perfectly noiseless. As our model states, the advantage of the additional tier arises because transcription is intrinsically noisy. Importantly, the enhancers of the pair-rule genes contain binding sites for both maternal and gap gene transcription factors, and likewise, many segment polarity gene enhancers bind gap, pair-rule, and maternal inputs [40, 41]. Our framework shows that these binding events may lead to increased precision in the control of

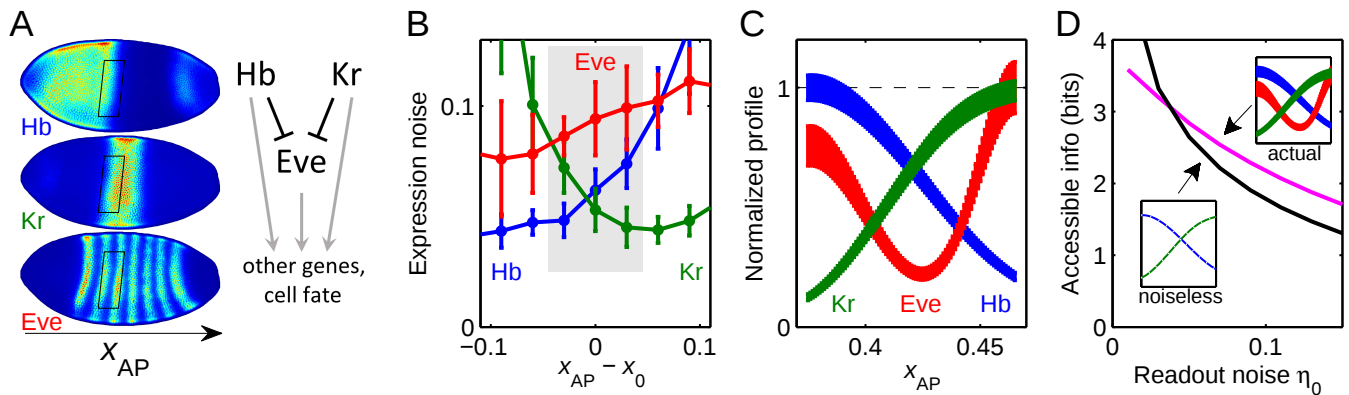


FIG. 4. **A:** Immunostaining of three antero-posterior (AP) axis patterning genes in the same embryo. Rather than specifying cell fate directly, the “gap genes” such as *hunchback* (Hb; top) and *Krüppel* (Kr; middle) control “pair-rule” genes such as *even-skipped* (Eve, bottom). Both tiers regulate other genes further downstream. Boxes indicate the selected region of interest (ROI), where at this time, Hb and Kr are the only relevant inputs to Eve, as shown on the cartoon. **B:** Within the ROI (shaded), Eve exhibits higher expression noise than either Hb or Kr. Expression noise computed as RMS difference between expression level of a nucleus and its immediate dorsal or ventral neighbor (see Methods), plotted against AP distance from the Hb/Kr boundary (denoted x_0). Error bars are standard deviation over $N = 8$ embryos. **C:** Idealized morphogen profiles, restricted to the ROI. Profile shape obtained as smooth spline-fit to expression values and noise magnitudes calculated for the profiles of panel A after projection onto the AP axis. **D:** For all but the lowest readout noise magnitude, joint accessible information content in the triplet (Hb,Kr,Eve) exceeds the accessible information provided by Hb and Kr alone, even in an extreme hypothetical case when they are rendered entirely noiseless.

gene expression, resulting in a higher level of accuracy than could be achieved in the absence of multiple tiers.

Discussion

Higher noise tolerance is a well-known advantage of digital signal processing. The *Drosophila* patterning network has been described as performing a “transition from analog to digital specification” of cell identity [32], but this “digital” metaphor has its limitations: even for Eve, the graded distribution within gene expression domains contains information [14]. Our work expresses this intuition in precise information-theoretic terms, and applies to any system in which initially identical cells process patterning information to generate distinct identities. Importantly, we have shown that an approach focusing solely on the raw information transmission through the network is insufficient to understand the functioning of the patterning system.

In our model, we assumed that fluctuations in $c(x)$ are uncorrelated between cells. In a real system, strongly correlated noise can be introduced, for example, by variations in the total amount of morphogen deposited maternally. These fluctuations, which cannot be reduced by averaging, lead to imperfect *reproducibility* of morphogen activity at a given location across multiple embryos. Much work has focused on investigating the limitations imposed on patterning by this type of fluctuations [14, 42, 43]. In contrast, our model is applicable for

understanding the effects of imperfect *precision* of gene expression (at a given location within the same embryo). The distinction between “raw” and “accessible” information does not rely on the assumption of uncorrelated noise.

It has been suggested that developmental circuits could be understood as solutions to some optimization problem. If so, what might they optimize? If the entire set of functional (cell-fate specific) genes were to be included into consideration, then information transmission from the input to this entire layer of functional genes would be a plausible objective function for this whole network to maximize, under some “bounded complexity” constraint penalizing solutions where hundreds of cell-fate specific genes are all controlled by highly complex enhancers with combinatorial, cooperative regulation.

However, the usual, more economical approach does not consider the full set of hundreds of cell-fate determining genes. Instead, it recognizes that the bulk of the patterning task is accomplished by a small subset of dedicated genes that engage in complex cross-regulation to establish the pattern that all other genes can then interpret simply. If we focus only on this core subset, the “economy of complexity” constraint is conveniently imposed by construction. We must realize, however, that maximizing information transmission to the target genes (downstream of the patterning core) imposes a different requirement onto this core circuit than merely efficient information transfer within the core itself. Instead, the core circuit must function as a format converter, re-encoding information at its input into a format that can

be accessed with a simpler and faster readout, that of a patterning cue by a functional gene.

Curiously, it has been shown that in small networks with a realistic model of noise, maximizing raw information transmission leads to network structures exhibiting features such as tiling of patterned range with amplifying input/output readouts [44–46], i.e. features that tend to also make information more accessible, even though the optimization scheme employed in these studies did not specifically consider the encoding format. This remarkable coincidence, however, should not obscure the fact that ultimately the two tasks — maximizing information transmission and re-encoding it in a more accessible format — could be conflicting.

Information theory is a powerful tool; its formalism does not, however, aim to replace considerations of what constitutes useful information or how it might be used by the system. As it is gaining popularity in biological applications, it is important to remember that for a channel $X \mapsto Y$, the relation between mutual information $I(X, Y)$ and the ability to use Y to determine X is only asymptotic: Shannon [13] proved that it is the maximum rate of error-free communication via this channel, *in the limit of infinite uses* of the channel. Importantly, in development and biological signaling, the number of channel uses (e.g. integration time of the signal) is fundamentally finite. Further, Shannon’s results assumed an encoder/decoder of infinite computational power [13]. This asymptotic rate is never in fact achieved in practice [47], but in biological context, performance is constrained even further, since the “encoding scheme” is usually limited to measuring the same signal multiple times. In communication theory, this bears the name of “repetition code” and is formally classified as a “bad code”, i.e. a code that does not attain Shannon’s bound even asymptotically. This means that extracting all the “raw” information from a signal is impossible even in principle. For example, a signaling pathway with capacity of 1 bit is never sufficient to make a reliable binary decision, and therefore should not be conceptualized as a binary switch.

As illustrated here, making the distinction between “raw” and “accessible” information will be crucial for understanding the architecture and function of patterning and signaling circuits. More work is required: our definition of accessible information relied on a simplistic noise model; in general, quantifying the usefulness of information-bearing signals in contexts where channel uses are limited will require reinstating considerations of rate/fidelity tradeoff, which Shannon could eliminate by taking the limit of infinite-time communication. Nevertheless, information theory remains a most adequate framework to address these issues, provided it is extended to quantify both the amount and accessibility of information. Our work provides a step in this direction and demonstrates how the extended framework naturally ex-

plains a global architectural property shared by diverse patterning circuits.

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- $$I_{\text{acc}}(\{c^{(1)}, c^{(2)}, \dots\}) \equiv I_{\text{raw}}(\{c^{(1)} + \eta^{(1)}, c^{(2)} + \eta^{(2)}, \dots\}).$$
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Supplementary Information

Information carried by a linear morphogen gradient

For a linear morphogen $c(x)$ spanning the range $[0, c_{\max}]$, with constant Gaussian noise σ_0 , the information content is given by

$$I_{\text{raw}}[c] \equiv I[c(x), x] = \ln \left(\frac{c_{\max}}{\sigma_0 \sqrt{2\pi e}} \right).$$

To show this, we apply the definition of the mutual information:

$$I[c(x), x] = H[P_c] - H[P_{c|x}]$$

Here P_c is the probability distribution of c (which is uniform between 0 and $c_{\max}$); $P_{c|x}$ is the conditional distribution of the concentration of c given x (which is Gaussian of width σ_0), and $H[P]$ is the differential entropy of a probability distribution P :

$$H[P] \equiv - \int P(z) \ln P(z) dz = - \langle \ln P \rangle_P.$$

Clearly, $H[P_c] = \ln c_{\max}$. The second term is the entropy of a Gaussian distribution P_{σ_0} of width σ_0 :

$$P_{\sigma_0}(z) = \frac{1}{\sqrt{2\pi\sigma_0^2}} \exp \left(-\frac{z^2}{2\sigma_0^2} \right)$$

and therefore:

$$\begin{aligned} H[P_{c|x}] &= - \langle \ln P_{\sigma_0}(z) \rangle_z = \ln \sqrt{2\pi\sigma_0^2} + \left\langle \frac{z^2}{2\sigma_0^2} \right\rangle_z \\ &= \ln \sqrt{2\pi\sigma_0^2} + \frac{1}{2} = \ln (\sigma_0 \sqrt{2\pi e}). \end{aligned} \quad (8)$$

Putting this together, we find:

$$I[c(x), x] = H[P_c] - H[P_{c|x}] = \ln \left(\frac{c_{\max}}{\sigma_0 \sqrt{2\pi e}} \right).$$

Experimental procedures

Antibody staining was performed using procedures and antisera described in [1] and [2]. Confocal microscopy was performed at 12 bit resolution on a Leica SP5 with a 20x HC PL APO NA 0.7 immersion objective at 1.4x magnified zoom using pixels of size 135 x 135 nm covering an area of 554x554 nm. For each embryo, 17 images slices were obtained at a z interval of 4 microns, spanning approximately 50% of embryo thickness. All data were collected in a single acquisition cycle using identical scanning parameters.

Estimating expression magnitude (image processing)

The immunostaining procedure described above yields confocal stacks of images where pixel intensity corresponds to the recorded fluorescence level. Stacks were converted into projected Hb, Kr and Eve images (such as displayed on Fig. 4A) as the maximum projection of Gaussian-smoothed frames. The width of the averaging kernel (8 pixels, corresponding to approximately 1 μm) was smaller than the radius of the nuclei, therefore for pixels close to the nucleus center the averaging volume was wholly within the nucleus. Smoothing frames prior to maximum projection ensured robustness against imaging noise.

In each of $N = 8$ embryos, the location of nuclei was identified manually. For each of the projected images (Hb, Kr and Eve), we recorded the highest intensity value within 5 pixels of nuclei center locations as the fluorescence intensity in that nucleus. Allowing for a 5-pixel “wiggle room” ensured robustness against registration errors across color channels, as well as against errors in the manual selection of nuclei center locations. The recorded intensity values were corrected for background autofluorescence by subtracting the mean intensity recorded in nuclei located in non-expressing regions of the embryo. The background-corrected fluorescence values reflect protein concentration, up to a proportionality factor (intensity of a fluorophore). The fractional measurement noise in estimating relative concentrations can be estimated as the standard deviation of pixel intensity values within a nucleus on the projected map. In their respective regions of expression, this standard deviation of Hb, Kr and Eve pixel intensity constituted $\approx 1\%$ of the expression

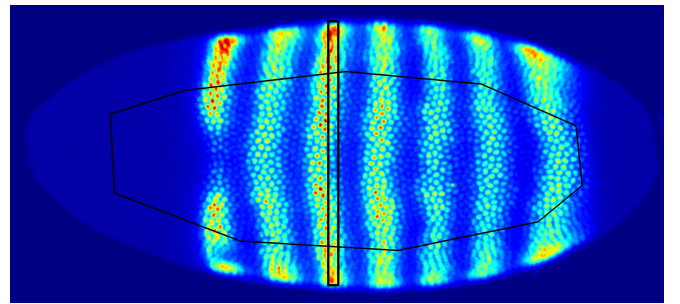


FIG. S1. Example of projected image (Eve). Black polygon indicates the analysis region, manually selected to exclude distorted areas close to the embryo edge. Rectangle indicates nuclei with the same projected coordinate onto the AP axis. Even in this perfectly ventral view of the embryo that minimizes the effects of stripe curvature (compare with Fig. 4A in the main text), the expression stripes are not exactly perpendicular to this axis.

value and was therefore negligible compared to the expression noise observed across nuclei (Fig. 4B). To avoid signal distortion artifacts observed at the edges of the imaged portion of the embryo due to tissue curvature and compression, all analysis was restricted to nuclei located in the low-distortion region selected manually along the imaged embryo center line, typically 20-25 nuclei wide (Fig. S1).

Estimating expression noise (Fig. 4B)

Expression noise is defined as:

$$c_{\text{noise}} = c_{\text{recorded}} - c_{\text{expected}},$$

where c_{recorded} is the recorded fluorescent intensity (of Hb, Kr or Eve), and c_{expected} is the expected value at that location. Measuring noise therefore requires a method for constructing c_{expected} . We use a method that we call “halter-shaped filtering”. To introduce and motivate this method, we begin by discuss two simpler alternatives and their limitations: binning by AP coordinate and neighbor averaging.

Binning by AP coordinate

Since gap genes expression is often said to be a function of the location along the antero-posterior (AP) axis, one approach could be to define c_{expected} as the average expression level in all nuclei with a similar AP coordinate. This approach, however, would yield strongly biased results due to the curvature of gene expression domains (Fig. S1).

Neighbor averaging

A better approach is to construct c_{expected} for each nucleus based on the expression levels observed in neighboring nuclei. Since expression profiles are relatively smooth functions of location, the average of expression levels in nuclei that are immediate neighbors of nucleus i provides a reasonable expectation for c_i . Despite being a significant improvement over the naive AP-based method, however, the simple averaging over neighbors provides an unbiased estimate only in regions where the profile shape is well approximated by a linear dependence. In all other cases this estimate will have a bias proportional to the convexity (second derivative) of the mean profile shape. This is particularly clear for the sharply varying profile of Eve (Fig. S2A). This bias can lead to a dangerous artifact, whereby sharply varying profiles would appear to be more noisy, which would be unacceptable for our analysis of the Hb-Kr-Eve system. Fig. S2B shows the

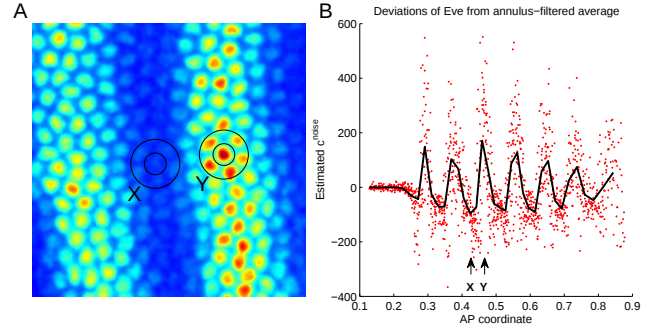


FIG. S2. The simple neighbor-averaging method will underestimate c_{expected} in the regions where the profile is concave, e.g. at the peaks of Eve stripes (nucleus X), and overestimate c_{expected} where the profile is convex, e.g. in the Eve troughs (nucleus Y). **A:** Eve stripes 2 and 3. Nuclei X and Y marked by smaller circles; the large circles encompass the neighbors over which averaging is performed. **B:** c_{noise} as estimated using the neighbor-averaging method, shown as a function of AP coordinate. Black line: window average of c_{noise} over 50 consecutive nuclei. This average should be close to zero for an unbiased estimate, but exhibits a clear correlation with the Eve profile shape.

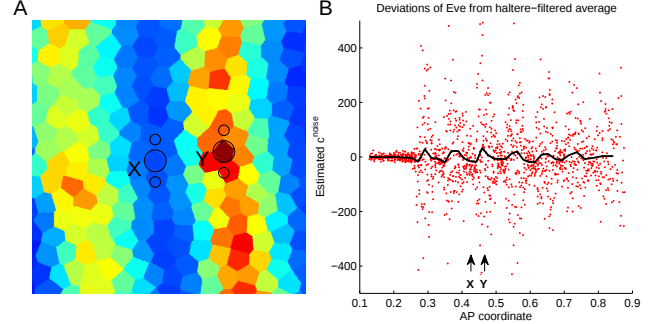


FIG. S3. **A:** “Eve map” of the region depicted in Fig. S2A, constructed as described in the text. X and Y label the same nuclei as in Fig. S2A; the larger circle marks their location. The smaller circles depict the haltere-shaped filter: c_{expected} is constructed as the average pixel value over this area around each nucleus. **B:** Inferred c_{noise} shown as a function of AP coordinate. The performance of the haltere-filtering method shows marked improvement compared to annulus filtering (Fig. S2B), as indicated by the greatly reduced fluctuations of the window-averaged c_{noise} (in black). The fact that the magnitude of c_{noise} increases in regions of greater expression is normal: larger expression means larger absolute noise.

inferred c_{noise} as a function of AP axis coordinate. The severity of the bias of the neighbor-averaging method of estimating c_{expected} can be measured by the clearly observed correlation between c_{noise} and the average profile shape of Eve (i.e. c_{recorded}).

Haltere-shaped filtering

We now describe the procedure we used to construct c_{expected} for our analysis. We begin by creating an “expression map” whereby in the projected image such as depicted in Fig. S1 the value of every pixel is replaced by the expression level c_{recorded} recorded in the nucleus closest to that pixel. The image is then filtered using a haltere-shaped filter depicted in Fig. S3A, and pixel values at each nucleus after filtering define the values of c_{expected} .

This method combines the better qualities of the two approaches discussed above. On a perfectly regular hexagonal lattice, this would be equivalent to the neighbor-averaging method using only the immediate dorsal and ventral neighbors, but the specific procedure we described naturally deal with lattice imperfections. In fact, c_{noise} in Fig. S2B was constructed using this exact procedure, but using an annulus-shaped filter depicted in Fig. S2A. Since the gradient of expression profiles is predominantly aligned with the AP axis, using a haltere-shaped filter greatly reduces any introduced bias (Fig. S3B).

One might expect that for even higher accuracy, the orientation of the haltere filter could be set not by perpendicularity to the imaginary AP axis, but by the iso-lines of the actual expression profile after sufficiently strong smoothing. However, in practice such an approach is functionally less robust due to the number of tunable parameters, and we empirically found the fixed-angle haltere filtering to result in the lowest bias as measured by the correlation of average c_{noise} in a region and the average c_{recorded} in that same region.

Idealized profiles (Fig. 4C)

The expression profiles of long body axis patterning genes in *Drosophila* form a pattern that, to a good approximation, can be considered one-dimensional. However, as discussed above, due to the curvature of expression profiles, x_{AP} is not the variable that best captures the variance. To estimate positional information in a gene expression pattern using data from single embryos, we therefore use the measured expression pattern shape and noise to construct what we call “idealized profiles”. First, we plot the recorded expression values c_{recorded} as a function of x_{AP} and construct a smooth spline fit that captures the mean profile shape; we denote the result $\mu(x_{\text{AP}})$. Next, the same procedure is applied to expression noise, estimated as described above: the smooth spline fit to c_{noise}^2 as a function of x_{AP} describes how the experimentally observed expression noise varies along the AP axis; we denote this root-mean-square deviation function $e(x_{\text{AP}})$. An expression pattern with mean $\mu(x_{\text{AP}})$

and independent Gaussian noise of magnitude $e(x_{\text{AP}})$ constitutes the “idealized profile” of a given patterning cue (see Fig. 4C).

Note that when calculating average noise magnitude for a given AP coordinate, expression noise is calculated as described in the previous section, i.e. *prior* to binning by AP. The result is the average of expression noise measured locally for all nuclei at a similar AP location — as opposed to the variance of expression among all nuclei at the same x_{AP} ; the latter, as we described, suffers from artifacts. The procedure we described effectively straightens out expression stripes: the resulting profile has the same mean and noise magnitude as observed experimentally, but is, by construction, a function of a single variable. This approach contrasts with the procedure of [1] where embryos were imaged in cross-section and only dorsal or ventral “expression profiles” were used, i.e. expression levels were recorded along a *particular* AP line (from multiple embryos). Here, we use *all* nuclei observed on a slightly flattened surface of a single embryo, and the variation of expression profile shape with the dorsal-ventral coordinate becomes a major factor.

Computing information content (Fig. 4D)

By definition, the information content (or the mutual information) $I(c, x)$ of a profile $c(x)$ is the average reduction of uncertainty of c after x becomes known:

$$I(x, c) = S(c) - \langle S(c|x) \rangle_x.$$

Here the first term is the entropy of the full distribution of c , which we denote P_c , and $S(c|x)$ is the entropy of the conditional distribution $P(c|x)$. We write:

$$P_c(c) = \int p(c|x)P_x(x) dx = \frac{1}{x_{\text{min}} - x_{\text{max}}} \int p(c|x) dx,$$

because the position x is uniformly distributed between x_{min} and x_{max} (in our case, $x_{\text{AP min}} = 0.37$ and $x_{\text{AP max}} = 0.47$).

These formulas express the information content of a one-dimensional profile entirely in terms of the conditional probability function $p(c|x)$. For the idealized profile, at a given AP location x_0 , the conditional distribution $p(c|x_0)$ is Gaussian with mean $\mu(x_0)$ and width $e(x_0)$; in particular, the entropy of $p(c|x_0)$ is known analytically. Therefore, we compute $I(x, c)$ by numerically performing the integral. We validated our code by computing information content of simple profiles for which the information content can also be calculated analytically.

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